

Reader Module 12 may also be used to visually monitor the chamber 20 to determine if or when an optimum quantity of sample has reached the chamber 20. The instructions can also direct the Reader Module 12, based on information provided through the container label 28, to use particular filters 58,66 appropriate for particular wavelengths, or to move the container 18
5 to particular positions to provide the Reader Module 12 access to particular fields, etc. When the test at hand calls for a chemical measurement, for example, the analytical algorithm identified through the label 28 will call for the measurements necessary to determine the optical density of the field. The concentration of the analyte can subsequently be calculated by the Programmable Analyzer 16 using an analysis algorithm that uses calibration data
10 communicated through the container label 28. For hematology analyses, on the other hand, an analysis algorithm may direct that a field be searched for images of a particular cell type for enumeration or evaluation purposes. The algorithm may direct that a single, most optimal field be considered, or most preferably that multiple fields be considered and the results be statistically analyzed to obtain a final statistically acceptable result. At one or more points during the analyses, the volume of the sample field may be determined, if required for the
15 analysis, and that data used in the final results calculation .

As stated above, the considerable utility of the apparatus 10 enables a wide variety of analyses to be performed of a single sample, using a single analytical container 18. The detailed examples given below are offered so that a complete appreciation of the present

20 invention apparatus may be gained.

Example 1: Hematological Analyses

Referring to FIG.4, to enable an analysis of white blood cells (WBC's) within an anticoagulated whole blood sample, a container 18 having approximately 0.8 micrograms (μ g) of a sensible colorant and 50 μ l of anticoagulated whole blood disposed within its reservoir 22
25 is inserted into the Sample Transport Module 14. Prior to insertion, the operator may gently shake the container 18 to ensure uniform mixing of the colorant and the fluid sample. The label reader 38 disposed within the Reader Module 14 reads the container label 28 and

transfers the information contained within the label 28 to the Programmable Analyzer 16. In this example, the information identifies one or more specific analysis algorithms to be used and a plurality of container features operable to enable the analysis of the biologic fluid sample.

Those features include identifying the anticoagulating agent as EDTA, the sensible colorant as

5 a fluorescent highlighting supravital stain such as acridine orange (or basic orange-21 or the like), and physical characteristics of the container chamber 20 and the spatial locations of those physical characteristics within the chamber 20. For this particular analysis, only the second wall 32 of the container chamber 20 need be transparent since a fluorescent stain is being used. In all cases, it is the features of the container 18 and the capabilities of the apparatus 10 to utilize those features that enables the apparatus 10 to perform a plurality of tests on a single sample.

Referring to FIGS. 3 and 4, the Programmable Analyzer 16 next directs the rod 90 within the Reader Module 12 to actuate the valve 26 within the container 18 and thereby release the sample and colorant mixture into the chamber 20. Once the sample is distributed within the chamber 20, the sample resides quiescently during the analysis. The only sample motion within the chamber 20 will possibly be Brownian motion of the sample's formed constituents, and that motion is non-disabling for the present invention. Using the information provided through the container label 28, the analysis algorithm directs the positioner 86 to move the container 18 to a position where the field illuminator 40 is aligned

20 with a first region of the chamber 20, and in particular with one of a plurality of fields having a through-plane thickness 78 of approximately twenty microns. The intra-chamber spatial location of each of these fields is known and communicated to the Programmable Analyzer 16 through the label 28. The chamber through-plane thickness 78 of approximately twenty microns is chosen for a couple of reasons. First, an evaluation volume of $0.02\mu\text{l}$, (formed by a particular sample field having a cross-sectional area of one millimeter (mm) and a through-plane thickness 78 of twenty microns) typically contains 50-200 WBC's which is a favorable quantity for evaluative purposes. The cross-sectional area referred to is the area of the sample

imaged by the field illuminator 40 as described above. Second, a through-plane thickness 78 of twenty microns provides an optimal chamber 20 for rouleaux and lacunae formation.

If the sample is imaged by the apparatus 10 immediately after the sample has been inserted into the chamber 20, the sample will appear opaque when examined with the epi-
5 illuminated fluorescence and will not be favorable for analysis. The opaque appearance is caused by the red blood cells (RBC's), which form an overlapping mass prior to the formation of the rouleaux. To avoid an undesirable opaque image, the analysis algorithm stored within the Programmable Analyzer 16 provides a timing function wherein operation of the field illuminator 40 is delayed for a period of approximately thirty (30) seconds after the sample
10 has been introduced into the chamber 20. During that time, the Programmable Analyzer 16 may position the appropriate SE or LSE filters 58,66 if any, within the path of the light beam
15 54 within the field illuminator 40. After the delay, light selectively produced from the light source 44 and filtered within the field illuminator 40 is directed into a sample field within the chamber 20. The light passing into the sample causes the colorant within the sample to fluoresce and emit light of a particular wavelength. The emitted light then passes through the field illuminator 40 and into the image dissector 42 where it is converted into an electronic format in real time.

The electronic format of the emitted image, which can be shown real-time on the monitor 102, will show that after lying substantially motionless for approximately thirty (30)
20 seconds within the chamber 20, the RBC's will have spontaneously clustered into a plurality of rouleaux separated by lacunae. It is in the lacunae where whole blood sample constituents other than RBC's (e.g., WBC's and platelets) can be found and evaluated. Using 0.02 μ l sample fields keeps the number of WBC's in each field reasonable (a normal whole blood sample contains approximately 7,000 WBC's per μ l of sample; a 0.02 μ l sample of normal
25 whole blood contains approximately 140 WBC's). A number of fields within the first region are evaluated until a statistically sufficient number of cells are counted, which in practice is approximately 1000 cells.